

# Fluid continuity equation simulation: Monitoring fluid reservoir volume in the heart over time

Olivia Maftukhaturrizqoh\*, Agung Dwi Wijaya, Iftita Ida Sofia, Mohtar Yunianto

Department of Physics, Universitas Sebelas Maret, Surakarta 57126, Indonesia

ABSTRACT	ARTICLE INFO

Fluid flowing in a cross-section of a channel follows the law of continuity, namely the mass rate of fluid entering will be the same as the mass rate of fluid leaving. One of the applications of fluid flow is in human blood flow. Blood flow is controlled by the heart which functions to pump blood to and from the heart. The flow of blood entering and leaving the heart is determined by the cross-sectional area of the channel and the speed of blood flow through the heart. The speed of blood flow in the heart consists of two speeds, namely the systolic speed when blood leaves the heart and the diastolic speed when blood enters the heart. So that the volume in the heart can be observed changes over time. By creating a simulation using the MATLAB programming language, the difference between normal heart volume and problematic heart volume can be known. A program called reservoir and cardiac based on graphical user interface was created to determine the volume of fluid in the reservoir at any time and compare the volume of fluid in normal and abnormal hearts concerning time in 1 systole-diastole cycle.

# Article history:

Received Nov 16, 2023 Revised Jan 20, 2024 Accepted Feb 23, 2024

#### Keywords:

Cardiac Fluid Heart MATLAB Reservoir

This is an open access article under the <u>CC BY</u> license.



# \* Corresponding Author

E-mail address: oliviamaftukha@student.uns.ac.id

# 1. INTRODUCTION

Fluid flowing in a cross-section of a channel follows the law of continuity, namely the mass rate of fluid entering will be the same as the mass rate of fluid leaving [1-5]. One of the applications of fluid flow is in human blood flow [6-8]. Blood flow is controlled by the heart which functions to pump blood to and from the heart [9-13]. The flow of blood entering and leaving the heart is determined by the cross-sectional area of the channel and the speed of blood flow through the heart [14-17].

The speed of blood flow in the heart consists of two speeds, namely the systolic speed when blood leaves the heart and the diastolic speed when blood enters the heart [18-21]. So that the volume in the heart can be observed changes over time [22-25]. The speed of systole and diastole is different for each individual, by simulating the heart volume against time in normal conditions and comparing it with certain conditions so that the differences can be observed it is hoped that it can be used to detect whether the blood flow can be categorized as normal or not so that it can be used to detect heart abnormalities. Simulation can make it easier to detect differences in the volume of a normal heart and a problematic heart through a program so that it is hoped that we can find out the problems that occur in the heart.

# 2. RESEARCH METHODS

Simulation of the fluid continuity equation by monitoring the volume in the reservoir and the fluid volume in the heart was created using the MATLAB programming language. MATLAB is a programming language that comes with functions and characteristics that are different from other existing programming languages.



Figure 1. Flowchart for the reservoir program.





MATLAB is a high-level programming language specifically for technical computing, visualization, and programming needs such as mechanical computing, data analysis, algorithm development, simulation and modeling as well as calculation graphics. This fluid continuity equation simulation program uses a numerical approach and uses the Euler method in its equations. This program is structured in several stages, namely gather information, create an algorithm, create a program design, create a program, validation, trial, and design improvements (see Figure 1 and 2).

# 3. RESULTS AND DISCUSSIONS

A MATLAB graphical user interface (GUI) based program has been created with the name reservoir as in Figure 3. The reservoir program is to simulate fluid volume versus time in a reservoir. From this program, we can know the volume of fluid in the reservoir at any time, the time when the reservoir is full, and so on.



Figure 3. Graph of fluid volume against time in a reservoir.



Figure 4. MATLAB GUI-based *cardiac.fig* program.

Meanwhile, to simulate the fluid volume in the heart, the *cardiac.fig* program in Figure 4 has been created, which is also based on the MATLAB GUI. In the GUI there are two graphs, namely a graph that simulates the volume of fluid in the heart against time with variable values for a normal heart without disorders (default). These variable values include systolic velocity, diastolic velocity, aortic diameter, vena cava diameter, pulmonary artery diameter, and pulmonary vein diameter. Meanwhile, in another graph, the volume of fluid in the heart is simulated with the values of these variables being changed.



Figure 5. Graph of fluid volume in a normal heart versus time in one systole-diastole cycle.

In Figure 5, the GUI section with variable values that can be changed is first filled in with the default values for a normal heart. The resulting two graphs produce the same curve, which shows that the program is running well. Then, the program enters variable values that are different from the default normal heart with the following Figure 6.





Science, Technology and Communication Journal, 4(2), 45-50, February 2024

Thus, with this program it is possible to compare the condition of the fluid volume in a normal heart and an abnormal heart in one systole-diastole cycle, that is, with the input variables changed according to the condition of the heart to be simulated.

# 4. CONCLUSION

The *reservoir.fig* program simulates fluid volume versus time in a reservoir. From this program, we can know the volume of fluid in the reservoir at any time, the time when the reservoir is full, and so on. The *cardiac.fig* program can simulate a graph of fluid volume in a normal and abnormal heart versus time in 1 systole-diastole cycle so that it can also be compared. This is done by filling in the input variables according to the condition of the heart to be simulated.

# REFERENCES

- [1] Anggraeni, D. P. & Widiyarti, P. A. (2017). Simulasi aliran darah dalam pembuluh darah manusia dengan metoda lagrange smooth particle hydrodynamic (SPH). *Electrician–Jurnal Rekayasa dan Teknologi Elektro*, **11**(2).
- [2] Bozlar, U. G. U. R., Ors, F., Deniz, O., Uzun, M., Gumus, S., Ugurel, M. S., ... & Tayfun, C. (2007). Pulmonary artery diameters measured by multidetector-row computed tomography in healthy adults. *Acta Radiologica*, 48(10), 1086–1091.
- [3] Douglas, J. F. (2006). *Fluid mechanics fifth edition*. England: Prentice Hall.
- [4] Shchelchkov, A. V., Fafurin, V. A., Korneev, R. A., & Tukhvatullin, R. R. (2022). Modification of the equation for mass flow rate (mass) measurement of liquid with account of dynamic influencing factors. *Flow Measurement and Instrumentation*, **83**, 102117.
- [5] Lou, W., Wang, Z., Zhang, J., Liu, H., Sun, B., & Zhang, F. (2023). Flow regime evolution mechanism and falling flux prediction model for bypass injection of viscous liquid in vertical T-junction. *Chemical Engineering Journal*, **476**, 146601.
- [6] Kim, Y. H., Marom, E. M., Herndon, J. E., & McAdams, H. P. (2005). Pulmonary vein diameter, cross-sectional area, and shape: CT analysis. *Radiology*, **235**(1), 43–49.
- [7] Raissi, M., Yazdani, A., & Karniadakis, G. E. (2020). Hidden fluid mechanics: Learning velocity and pressure fields from flow visualizations. *Science*, **367**(6481), 1026–1030.
- [8] Ellahi, R., Zeeshan, A., Hussain, F., & Asadollahi, A. (2019). Peristaltic blood flow of couple stress fluid suspended with nanoparticles under the influence of chemical reaction and activation energy. *Symmetry*, **11**(2), 276.
- [9] Mboi, N. (2013). Panduan peringatan hari kesehatan sedunia. Jakarta.
- [10] Munson, D. F. Y. (2005). Mekanika Fluida edisi ke-4. Jakarta: Erlangga.
- [11] Oertel, H. & Krittian, S. (2011). *Modelling the human cardiac fluid mechanics*. German: KIT Scientific Publishing.
- [12] Courchaine, K., Rykiel, G., & Rugonyi, S. (2018). Influence of blood flow on cardiac development. *Progress in biophysics and molecular biology*, **137**, 95–110.
- [13] Ovsenik, A., Podbregar, M., & Fabjan, A. (2021). Cerebral blood flow impairment and cognitive decline in heart failure. *Brain and Behavior*, 11(6), e02176.
- [14] Streeter, V. L. & Prijono, A. (1988). Mekanika Fluida (terjemahan). Jakarta: Erlangga.
- [15] Saktioto, S., Defrianto, D., Thoibah, A., Soerbakti, Y., Syahputra, R. F., Syamsudhuha, S., Irawan, D., Hairi, H., Okfalisa, O., & Amelia, R. (2023). Simplified kinetic model of heart pressure for human dynamical blood flow. *Indonesian Journal of Electrical Engineering and Informatics (IJEEI)*, **11**(3), 870–882.
- [16] Mestre, H., Tithof, J., Du, T., Song, W., Peng, W., Sweeney, A. M., ... & Kelley, D. H. (2018). Flow of cerebrospinal fluid is driven by arterial pulsations and is reduced in hypertension. *Nature Communications*, 9(1), 4878.
- [17] Enjalbert, R., Hardman, D., Krüger, T., & Bernabeu, M. O. (2021). Compressed vessels bias red blood cell partitioning at bifurcations in a hematocrit-dependent manner: Implications in tumor blood flow. *Proceedings of the National Academy of Sciences*, **118**(25), e2025236118.
- [18] Meschini, V., Viola, F., & Verzicco, R. (2020). Heart rate effects on the ventricular hemodynamics and mitral valve kinematics. *Computers and Fluids*, **197**, 104359.

- [19] Dedè, L., Menghini, F., & Quarteroni, A. (2021). Computational fluid dynamics of blood flow in an idealized left human heart. *International Journal for Numerical Methods in Biomedical Engineering*, **37**(11), e3287.
- [20] Viola, F., Meschini, V., & Verzicco, R. (2020). Fluid-structure-electrophysiology interaction (FSEI) in the left-heart: a multi-way coupled computational model. *European Journal of Mechanics-B/Fluids*, **79**, 212–232.
- [21] Wang, F., Jin, P., Feng, Y., Fu, J., Wang, P., Liu, X., Zhang, Y., Ma, Y., Yang, Y., Yang, A., & Feng, X. (2021). Flexible Doppler ultrasound device for the monitoring of blood flow velocity. *Science Advances*, 7(44), eabi9283.
- [22] Saktioto, T., Soerbakti, Y., Thoibah, A., Meyzia, B., Syahputra, R. F., Irawan, D., & Hairi, H. (2023). Numerical investigation of physical parameters in cardiac vessels as a new medical support science for complex blood flow characteristics. *Baghdad Science Journal*, 20(6), 2322–2329.
- [23] Haryadi, H., Sugianto, S., Mahmudi, A., & Kartanegara, R. S. (2022). A numerical study on T-reduce junction flow distribution. *Science, Technology and Communication Journal*, 2(2), 55–62.
- [24] Hallow, K. M., Helmlinger, G., Greasley, P. J., McMurray, J. J., & Boulton, D. W. (2018). Why do SGLT2 inhibitors reduce heart failure hospitalization? A differential volume regulation hypothesis. *Diabetes, Obesity and Metabolism*, **20**(3), 479–487.
- [25] Zhang, Z., Yang, L., & Zheng, Y. (2018). Translating and segmenting multimodal medical volumes with cycle-and shape-consistency generative adversarial network. *Proceedings of the IEEE conference on computer vision and pattern Recognition*, 9242–9251.